



# Learning Algorithms for Medical Image Analysis

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# Outline

1. learning-based strategies for quantitative image analysis
2. automatic “annotation” of MR images: the example of synovitis assessment
3. data-driven image representation: *sparse coding* and *dictionary learning*
4. experiments and results

# Our Research in Medical Image Analysis

- ▶ Definition of new **“imaging biomarkers”** and design of algorithms for their assessment.
  - ▶ A biomarker is a “*characteristic that is objectively measured* and evaluated as an indicator of normal biological processes, pathogenic processes, or pharmacologic responses to a therapeutic intervention”
  - ▶ An imaging biomarker is, by extension, a biomarker measured from images.

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  1. Annotation and classification of image parts (i.e. single voxels or 2D/3D patches.)
  2. Non-rigid image registration, with specific interest for novel approaches to deal with discontinuous deformation fields.

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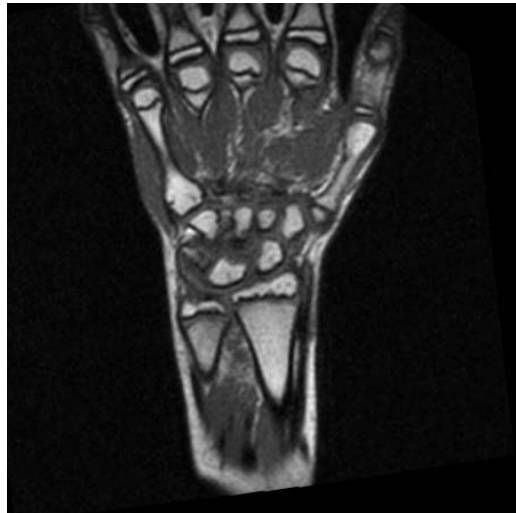
## Why learning from examples?

- ▶ *It is difficult to “translate” into an explicit algorithm the process of physicians’ diagnosis making.*
- ▶ *To ask the physicians to annotate images as positive or negative examples is a viable alternative that may lead to implicit learning-based algorithms.*

# The Challenges We are Currently Facing

- ▶ *quantitative analysis*  $\implies$  how to design efficient representation schemes to make the analysis more accurate?
- ▶ *large collections of 3D images*  $\implies$  how to design efficient and reliable learning algorithm for large scale problems?
- ▶ *weakly annotated data*  $\implies$  how to combine supervised and unsupervised learning approaches?
- ▶ *anatomical constraints*  $\implies$  how to exploit prior knowledge about known properties of tissue and organs?

# Automatic Assessment of Synovial Volume



## Setting

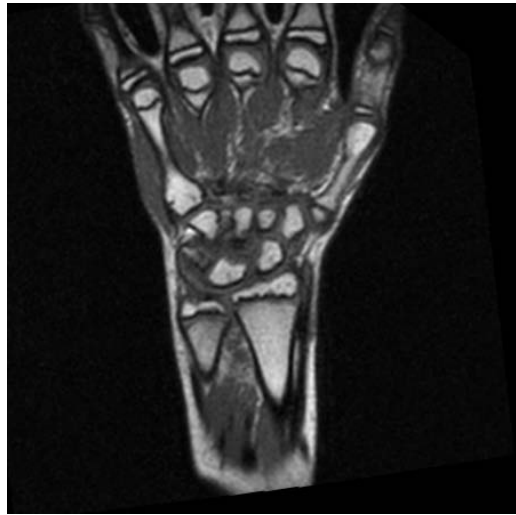
**Patients:** children under 16, affected by Juvenile Idiopathic Arthritis.

**Goal:** to measure the volume of the inflamed synovia, and investigate its use as a viable biomarker.

**Data:** 3D MR images acquired before and after the injection of a contrast medium.

**Context:** <http://health-e-child.org>

# Automatic Assessment of Synovial Volume



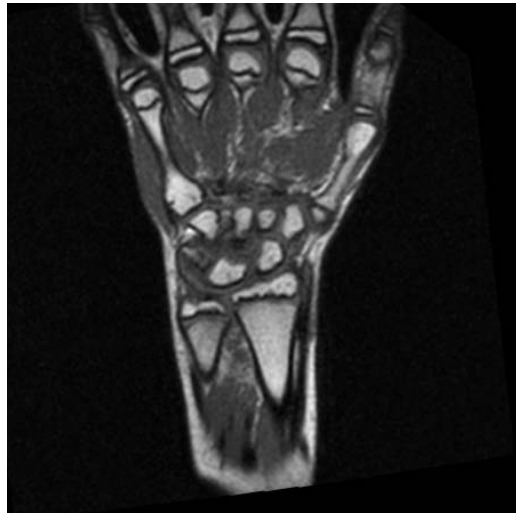
## The naïve approach

Given  $n$  voxels  $\mathbf{x}_i \in \mathbb{R}^d$  and the corresponding labels  $y_i \in \{+1, -1\}$ , the “optimal” solution may be computed as:

$$f(\mathbf{x}) = [K(\mathbf{x}, \mathbf{x}_1), \dots, K(\mathbf{x}, \mathbf{x}_n)] \cdot [(\mathbf{K} + n\tau\mathbf{I})^{-1} \mathbf{y}]$$



# Automatic Assessment of Synovial Volume



## Problems

- ▶ nonlinear methods may have storage and performance problems when  $n$  becomes large;
- ▶ data representation is often heterogeneous (e.g. measurements coming from different modalities):

$$\mathbf{x} \rightarrow \phi(\mathbf{x}) = \{\varphi^1, \dots, \varphi^k\}$$

# Multi-cue Voxel Classifier

We look for a more flexible discriminant function:

$$f(\phi) = \sum_{(i,j) \in \mathcal{I}} \alpha_i^j K_i^j(\phi) + b.$$

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## Assumptions

The  $k \times n$  basis functions

$$K_i^j(\phi) = \exp \left\{ -\frac{\|\varphi^j - \varphi_i^j\|^2}{2\sigma_j^2} \right\},$$

measure the similarity between  $\phi$  and one of the exemplar voxels with respect to a specific cue.

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## Model Selection

The **optimal subset**  $\mathcal{I}$  of basis functions, on which  $f$  depends, may be inferred directly from the data by means of a suitable feature selection algorithm.

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## Learning Algorithm

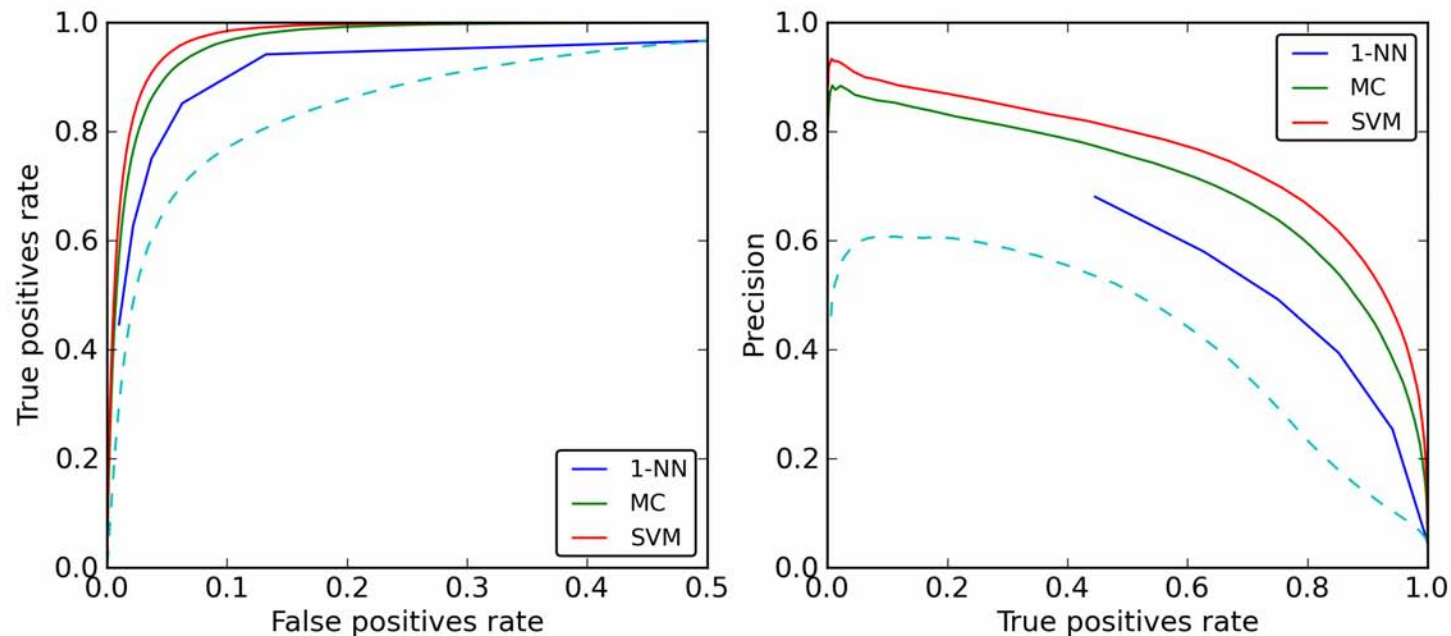
The goal of learning is to find the **optimal affine combination** defined by the coefficients  $\alpha_i^j$  and  $b$ .

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## Results



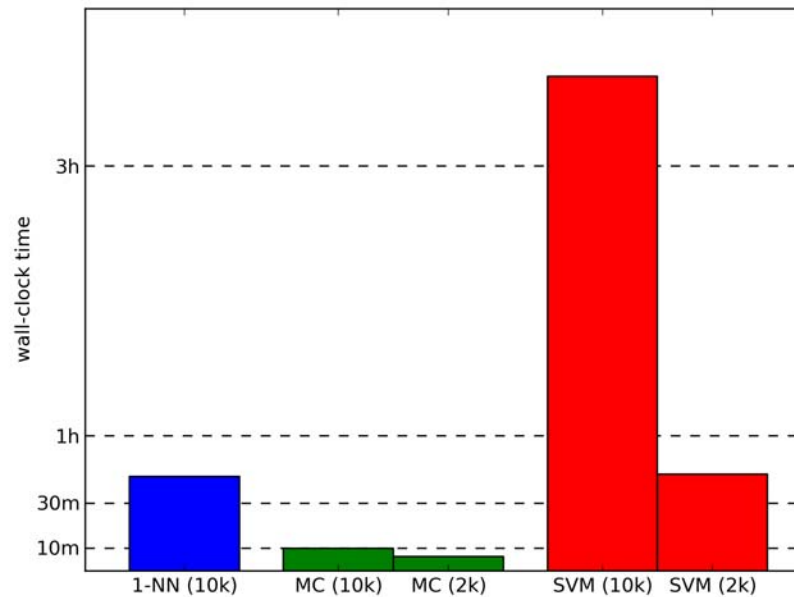
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## Results

- ▶ multi-cue classifier is **15+ times sparser** than SVM,
- ▶ and approximately **40 times faster** than SVM.



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## Results

- ▶ excellent accuracy and agreement with the manual measurements
- ▶ precision close to the one achieved by manual annotation
- ▶ positive preliminary results with both longitudinal and cross-sectional clinical studies.



# Data-driven Image Representation

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## 1. *vector quantisation*:

$$\mathbf{u}_i = j \text{ such that } \|\mathbf{x}_i - \mathbf{D}\mathbf{e}_j\| \leq \|\mathbf{x}_i - \mathbf{D}\mathbf{e}_k\| \forall k \neq j$$

## 2. *convolution*:

$$\mathbf{u}_i = \mathbf{D}^T \mathbf{x}_i$$

## 3. *sparse coding*:

$$\min_{\mathbf{u}_i} \{ \|\mathbf{x}_i - \mathbf{D}\mathbf{u}_i\|^2 + \lambda \|\mathbf{u}_i\|_1 \}$$

# Sparse Coding

- ▶ A signal may be conveniently represented as the superposition of elementary signals, or *atoms*.
- ▶ Over-complete dictionaries (or *frames*) and sparse coding offer more flexibility and are supported by successful applications.
- ▶ *Tight frames* ensure that the optimal representation can be recovered by means of inner products of the signal and the dictionary.

## Learning the dictionary from data

We investigated the possibility of learning directly from data a dictionary endowed with properties similar to that of tight frames.

# Dictionary Learning

## Setting

- ▶  $\mathbf{X} = [\mathbf{x}_1, \dots, \mathbf{x}_N] \in \mathbb{R}^{d \times N}$  is the *input* matrix.
- ▶  $\mathbf{U} = [\mathbf{u}_1, \dots, \mathbf{u}_N] \in \mathbb{R}^{K \times N}$  is the *coding* matrix.
  
- ▶ The goal is to learn:
  1.  $\mathbf{D} = [\mathbf{d}_1, \dots, \mathbf{d}_K] \in \mathbb{R}^{d \times K}$  (the *decoding* or *synthesis* operator), whose columns are the atoms of the dictionary, and
  2.  $\mathbf{C} = [\mathbf{c}_1, \dots, \mathbf{c}_K]^T \in \mathbb{R}^{K \times d}$  (the *encoding* or *analysis* operator), whose rows are filters that can be convolved with an input signal to obtain its encoding.

# Dictionary Learning

## Objective

We aim at learning both  $\mathbf{D}$  and its dual  $\mathbf{C}$  by minimising:

$$\begin{aligned}\mathcal{E}(\mathbf{D}, \mathbf{C}, \mathbf{U}) &= \frac{1}{d} \|\mathbf{X} - \mathbf{D}\mathbf{U}\|_F^2 + \frac{\eta}{K} \|\mathbf{U} - \mathbf{C}\mathbf{X}\|_F^2 + \frac{2\tau}{K} \sum_{i=1}^N \|\mathbf{u}_i\|_1, \\ s.t. \quad &\|\mathbf{d}_i\|^2, \|\mathbf{c}_i\|^2 \leq 1\end{aligned}$$

where  $\tau > 0$  is a regularisation parameter inducing sparsity in  $\mathbf{U}$ , while  $\eta \geq 0$  weights the coding error with respect to the reconstruction error.

# Dictionary Learning

## The Proposed Algorithm: PADDLE

The functional  $\mathcal{E}$  is separately convex in each variable, and we adopt a block coordinate descent strategy:

1. *sparse coding* step:  
minimise first with respect to the encoding variables  $\mathbf{U}$ , and then
2. *dictionary update* step:  
minimise with respect to the dictionary  $\mathbf{D}$  and its dual  $\mathbf{C}$ .

Each step is based on *proximal methods*.

The algorithm has been proved empirically successful, and its convergence towards a critical point of  $E$  may be proved.

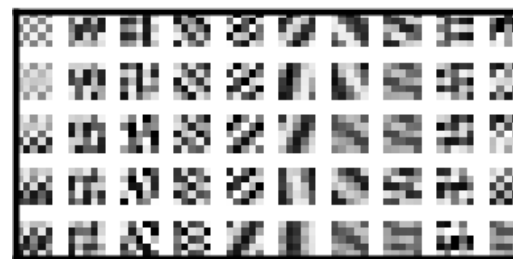
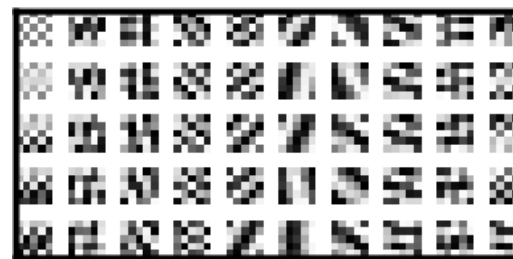
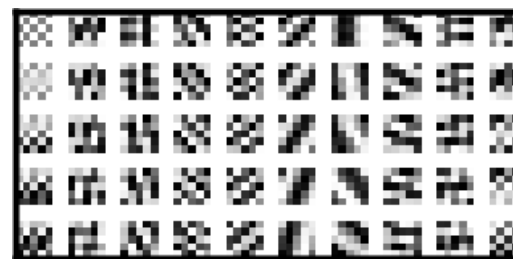
# Experimental Assessment

## Synthetic Data

Data have been generated as random superpositions of a small number of elements of a tight frame.

The reconstruction error has reached immediately the minimum achievable with the true generating frame.

From top to bottom, we show the original dictionary, the recovered dictionary  $\mathbf{D}$  and recovered dual  $\mathbf{C}^T$ .



# Experimental Assessment

## Benchmark Datasets

### **Berkeley segmentation dataset**

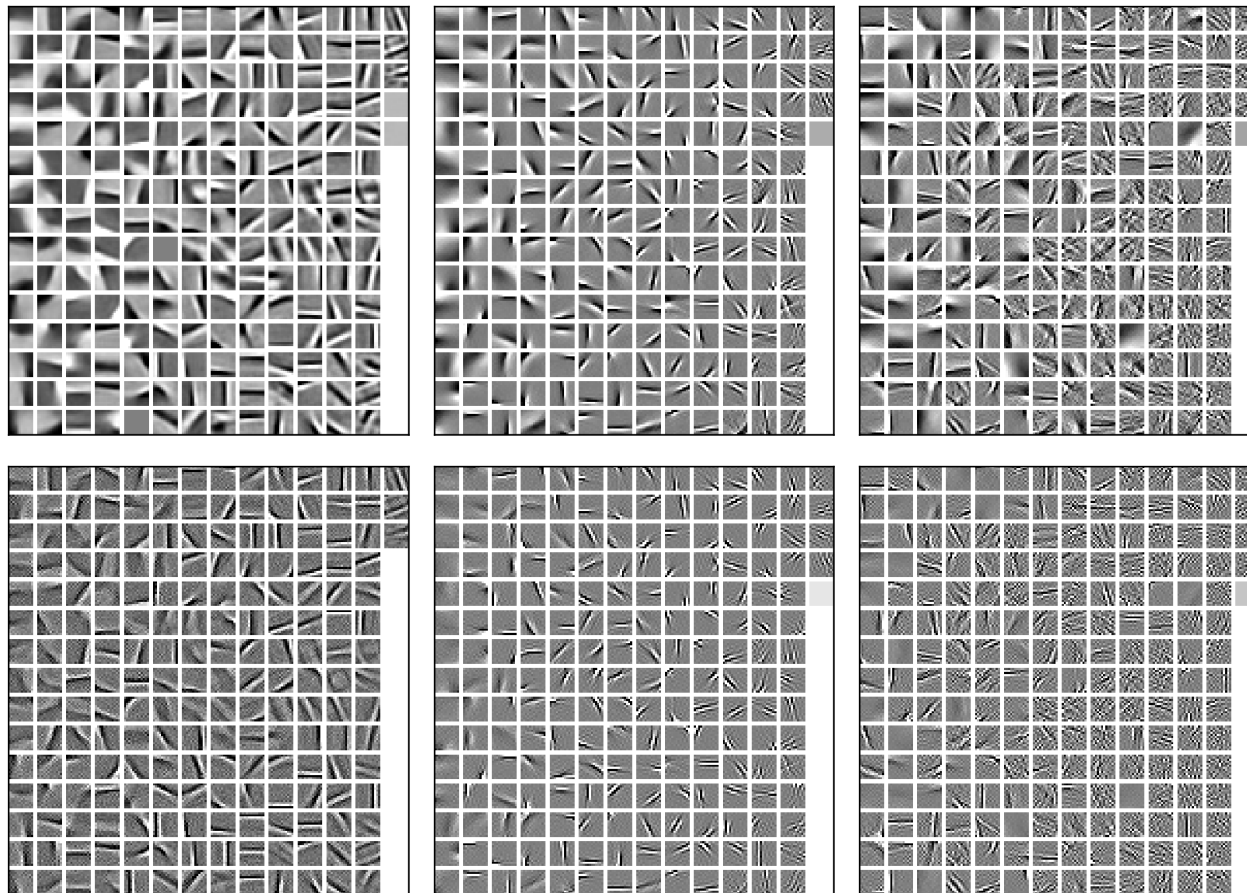
- ▶ we have extracted a random sample of  $10^5$  patches of size  $12 \times 12$  from the natural images contained in the dataset
- ▶ the reconstruction error achieved at the various level of sparsity have been constantly lower than the reconstruction error achievable with a comparable number of principal components



# Experimental Assessment

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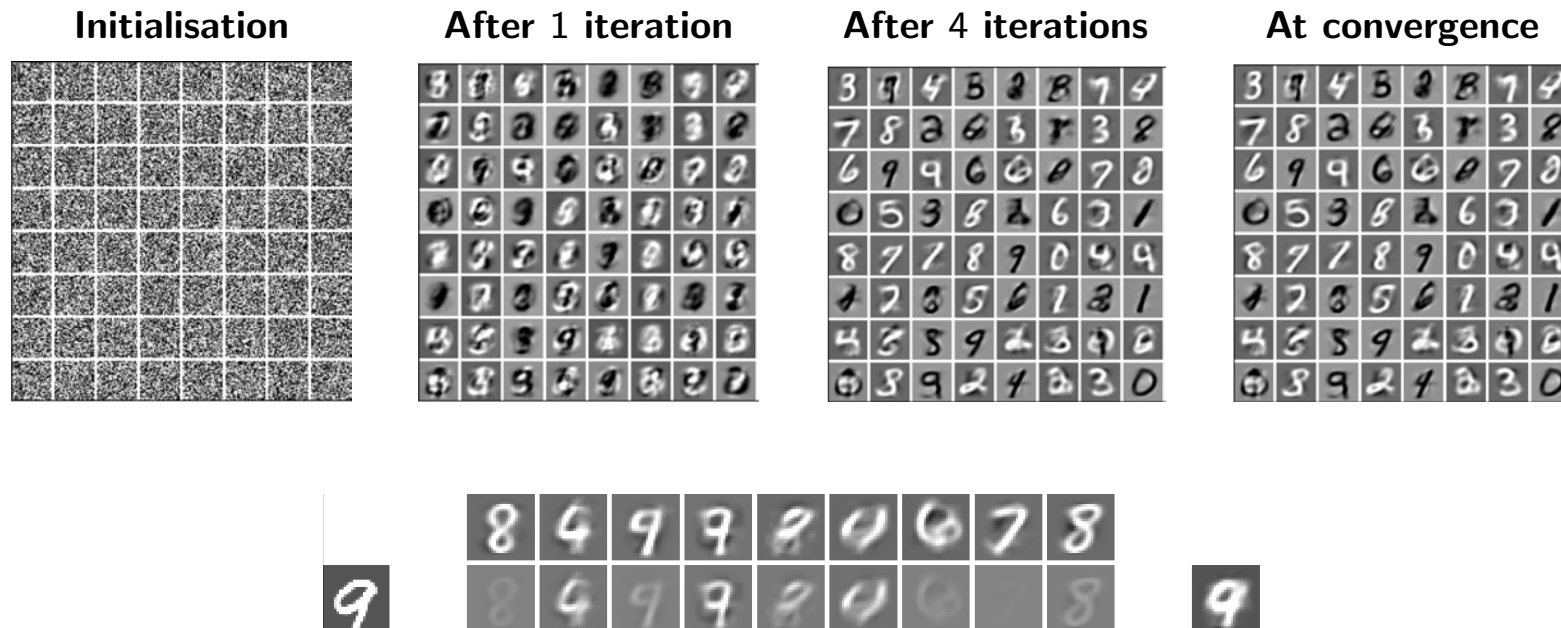


# Experimental Assessment

## Benchmark Datasets

### MNIST dataset

- ▶ we have tested the algorithm on the 50,000 training images consisting of  $28 \times 28$  quasi binary images of handwritten digits
- ▶ we have trained the dictionary with 200 atoms

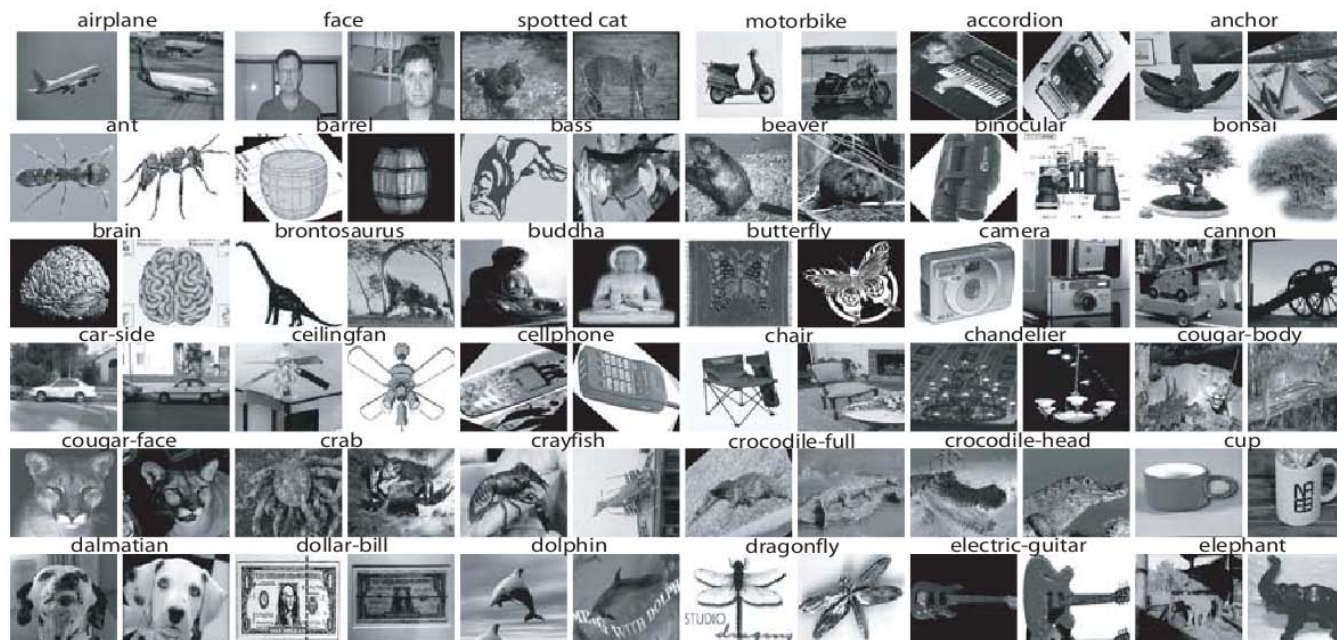


# Experimental Assessment

## Object Class Identification

### Caltech101 Dataset

- ▶ we have investigated the discriminative power of the dictionaries **D** and **C** when used to represent the visual content of an image



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- ▶ the performance obtained by using **C** is essentially the same as the one obtained with **D**.

	Coding based on D	Coding based on C	State-of-the-art results
<i>Mean accuracy</i>	0.987	0.984	0.985
<i>Standard deviation</i>	0.008	0.008	0.008

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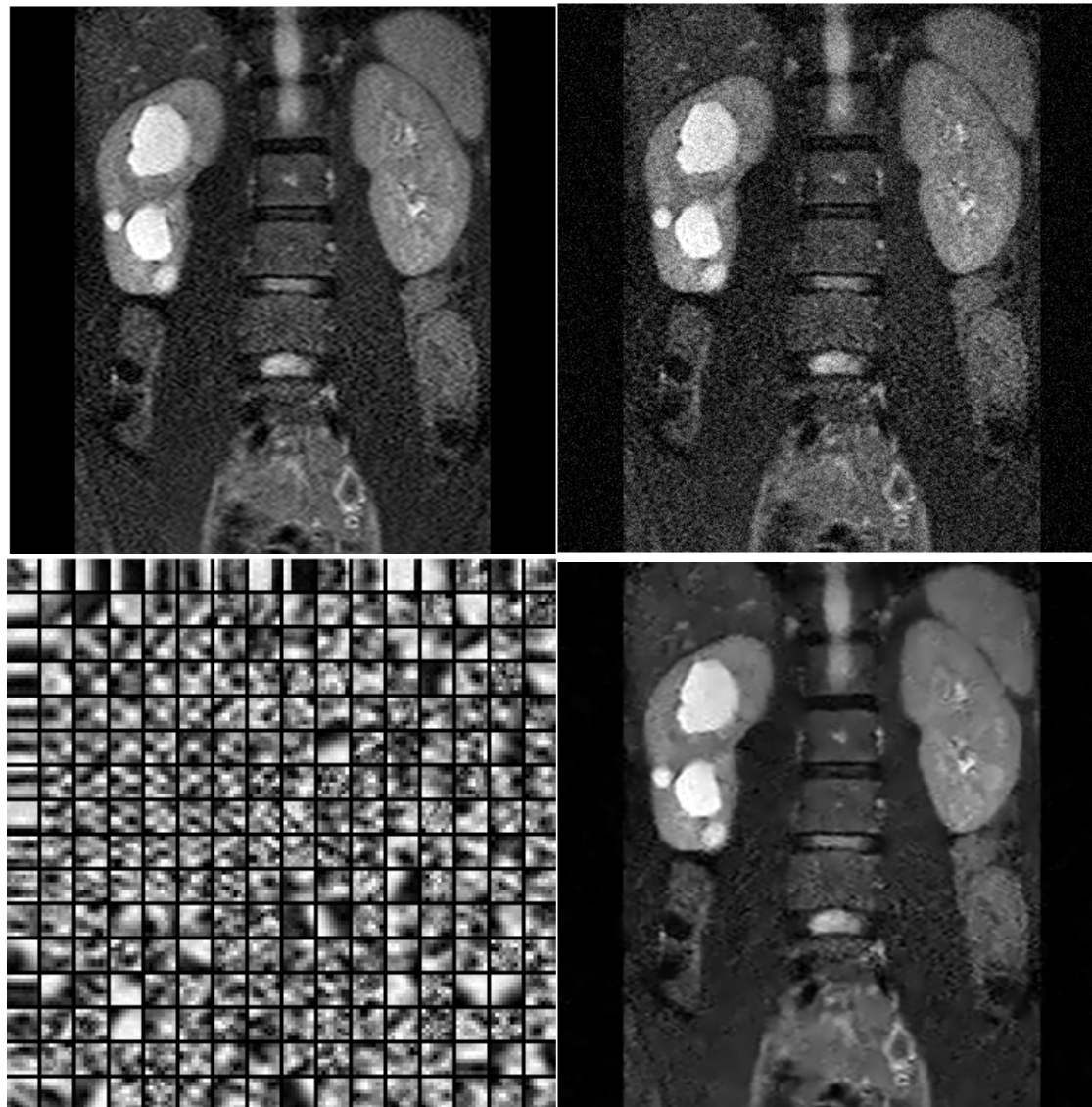
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- ▶ the coding of new input images requires only a matrix-vector multiplication.



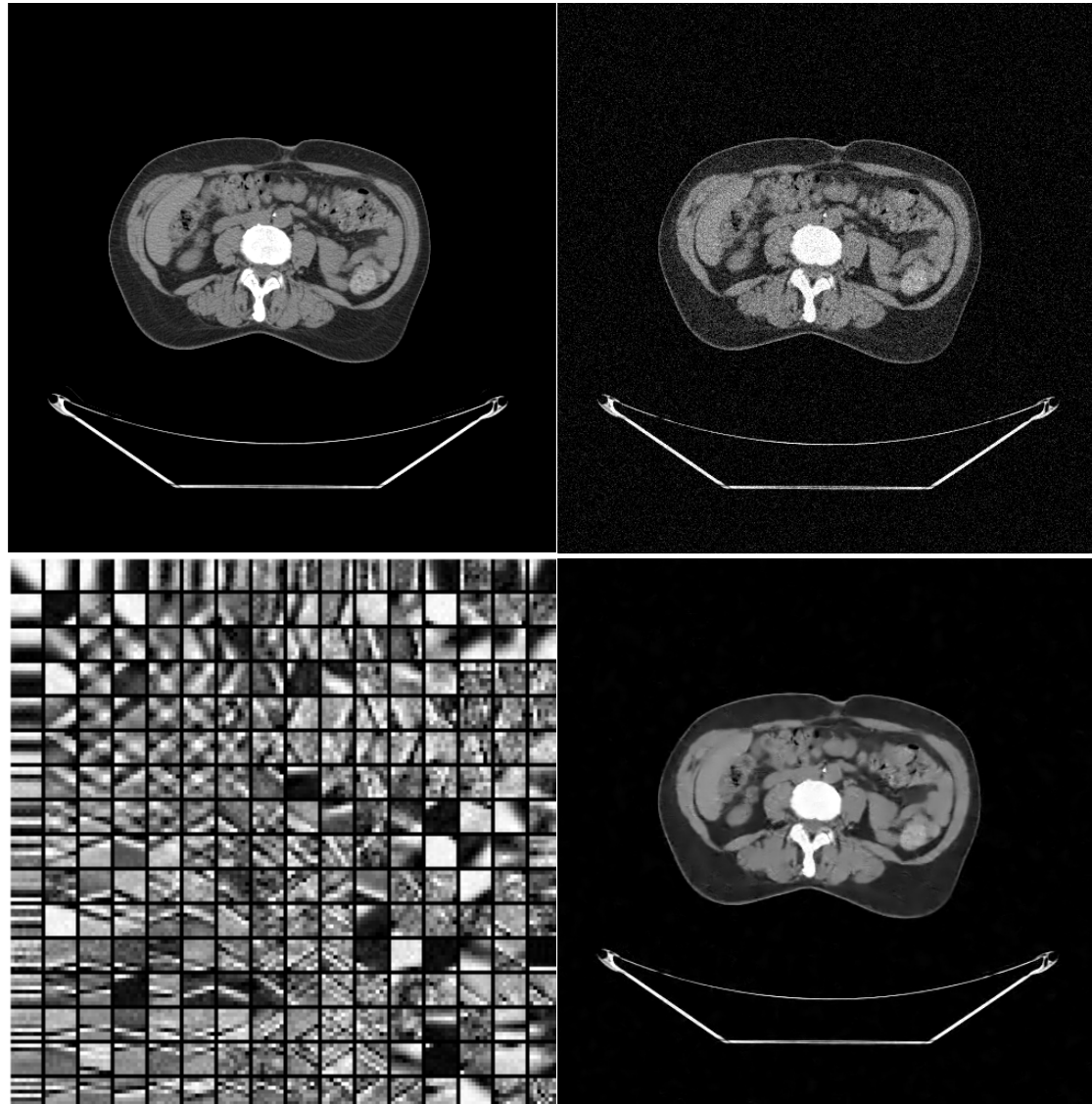
# Experimental Assessment

## Image Denoising



# Experimental Assessment

## Image Denoising



# References

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